

# Evaluation of the balance capabilities of elderly people rising in the longitudinal direction

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## Abstract

In this study, balancing capability in the longitudinal direction during rising from seated position was evaluated for the elderly. In particular, influence of rising speed at the moment of leaving the seat, referred to here as the "seat-off," on balancing capability was examined, since it affects the occurrence of falls. Twenty eight elderly individuals were participated in the study, and they were divided into two groups based on their experience of falls in the past: 19 in the stable rising group and 9 in the unstable rising group. Body movement and corresponding ground reaction forces during rising motion at two different speeds were measured for each subject using a motion capture system and a force plate, respectively, from which "seat-off parameters" that could characterize seat-off motion were obtained. Seat-off parameter values for the stable and unstable rising groups were separately distributed in the seat-off parameter space, forming two distinguished clusters. It was shown that the cluster for the unstable rising group was further divided into two sub-clusters. The result implies two types of instability during rising from seated position: an instability in the forward direction group and instability in the backward direction.

**Keywords:** the balancing capabilities in the longitudinal direction, seat-off parameters, fall.

## 1. Introduction

According to the 2014 Ministry of Health, Labour and Welfare's comprehensive Survey of living conditions, elderly having come to need assistance or nursing care in life have been reported as making up more than 14 percent of those injured in falling incidents[1]. As the ability to control the body reduces due to aging and degeneration, the risk of falling at the time of rising is higher. In addition, when entering a vicious circle of constantly repetitively falling, the daily-life ability of the elderly is significantly limited [2-7].

Therefore, to support the independent daily life of the elderly by preventing falling in advance, it is important to prevent the vicious cycle of falling regularly and repetitively [8]. In addition, preventing people from requiring care or assistance after falling, not only elderly people, is a major problem that is currently being faced by society, and is a trait characteristic of an ultra-aging society [9-10]. Furthermore, according to a report by the Ministry of Health, Labour and Welfare on falling mechanisms of the elderly, there appears to be a higher frequency of falls while standing or walking [1]. Among these, it is difficult to determine the specific reason because the amount of motion parameters is too large. These parameters include environmental problems and regulations for performing operations to diagnose the falling direction during walking.

However, it is considered to be possible to identify the tipping direction during rising, rather than during

walking since the amount of aforementioned parameters is comparatively limited [11]. In other words, there are kinematic and the dynamic analyses for grasping the balance capability during rising of the elderly, and it is possible that aid for preventing falling can be offered by predicting the direction which people tend to fall.

Conducting studies on rising behaviors in the past, including seat angles, changes in sitting posture, etc. have been pursued to explore the reactivity of a subject to changes in external environmental factors [12-15]. Actual causes of falls of elderly people, rather than simply looking at the external environment, have been performed in smaller numbers, due to the difficulty of the elder's unconscious environment being different from normal.

For example, in the case of the elder being in an excited state or in the case that the elder possesses a strong desire to void, by hurrying to get up faster than usual, or oppositely in a situation of decreased arousal, rising is slower than usual. Thus emotional and physiological concerns might have a significant effect on the stability of rising. If this rising speed exceeds the allowable capacity of the elder's own rising speed, and there is a change in the person's attitude control ability in response to rising up speed, the rising action is thought to become unstable.

In this study, the internal environment as well as the external environment was examined in order to evaluate how the longitudinal balancing capability at varying rising speeds greatly affect the fall in rising [16]. In particular, longitudinal balancing capability at

1 seat-off, which was associated with falls, was examined  
 2 closely [17-18]. As a measure of the longitudinal bal-  
 3 ancing capacity at the time of seat-off, seat-off param-  
 4 eters consisting of Center Of Gravity (COG)-heel hori-  
 5 zontal distance and COG horizontal velocity at the time  
 6 of seat-off, and at the same time measure the floor reac-  
 7 tion force were created and examined.

## 2. Method

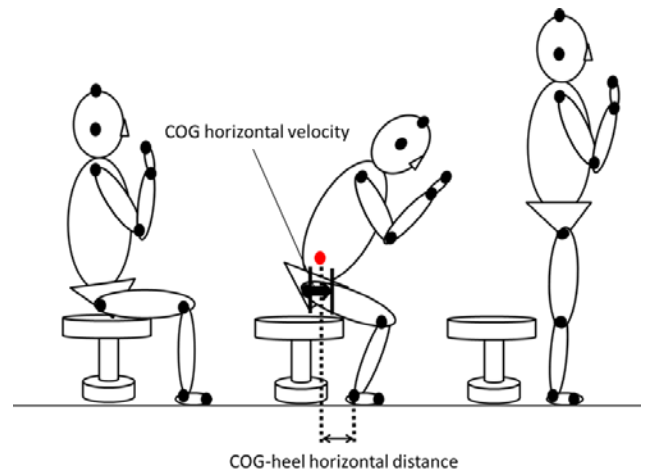
10 Subjects were 28 healthy elderly people of ages 74-92  
 11 that are residents in an elderly care house (13 males, 15  
 12 females). ADL of all subjects was self-level, including  
 13 the outing. Of the elderly 28 people, 9 people had a  
 14 history of falling more than 2 times (4 male, 5 female).  
 15 These people were grouped into the unstable rising  
 16 group. The other 19 people were grouped into a stable  
 17 rising group, and the following experiments were per-  
 18 formed. In addition, this study was approved by the  
 19 Okayama University Ethics Committee (approval No.  
 20 1824), all subjects received an adequate description of  
 21 the experiment, and only participated in the experiment  
 22 after formally agreeing to.

23 For the experiment, an armrest free chair, with a  
 24 seat height equivalent to the lower leg length of the  
 25 subject was used. The starting limb position was a static  
 26 sitting posture defined as having a hip-knee-ankle joint  
 27 angle of 90°, and allowed the subjects trunk to remain  
 28 in the vertical position as best as possible. The end limb  
 29 position was the still standing posture in which the head  
 30 and trunk are held in a vertical position. In addition,  
 31 both hands were placed in front of the chest, a legs  
 32 apart movement was not allowed. Just before the start  
 33 of the rising motion, one of the challenges, of being  
 34 either "fastest" or "slowest" was taught randomly and  
 35 the rising operation was performed five times, respec-  
 36 tively.

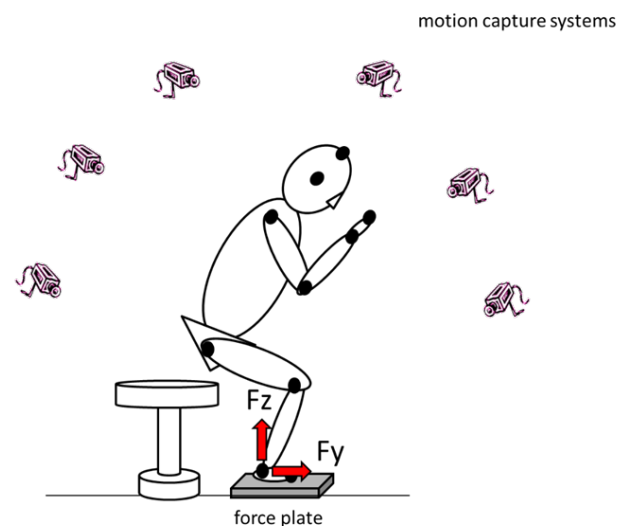
37 Image data of the subject at two speeds of rising  
 38 movement were acquired and analyzed by a motion  
 39 capture system (Move-tr./3D, library). The sampling  
 40 rate of the images was captured using image analysis  
 41 software at 50fps, the created seat-off parameters con-  
 42 sisting of COG-heel horizontal distance and COG hori-  
 43 zontal velocity at the time of seat-off were analyzed,  
 44 and the width of seat-off parameters between 2 task  
 45 were calculated, in order to examine their association.

46 Markers at, parietal, both ear holes, both acromi-  
 47 ons, both humerus lateral epicondyles, both radial sty-  
 48 loids, both third finger apexes, both greater trochanters,  
 49 both knees cleft center, both malleolus lateralis, and  
 50 both head of fifth metatarsals, were affixed to a total of  
 51 18 locations. To calculate the synthesized body's center  
 52 of gravity, in addition to these marker points, the head  
 53 point, breast point and waist point were defined as fol-  
 54 lows: The head point: the midpoint of the left and right  
 55 ear hole markers. The chest point: the midpoint be-  
 56 tween the left and right acromion markers. The waist  
 57 point: the midpoint of the left and right of the greater

58 trochanter markers. The timing of seat-off was deter-  
 59 mined by moving image data captured in the analysis  
 60 software by frame advance reproduction.  
 61 The COG-heel horizontal distance at the moment of  
 62 seat-off was defined as the horizontal distance between  
 63 a part of the supporting basal plane malleolus lateralis  
 64 and the body's center of gravity. The COG horizontal  
 65 velocity at seat-off was defined as the average velocity  
 66 of the preceding frame and one following frame, which  
 67 were calculated (Fig. 1). The horizontal and vertical  
 68 component forces at the time of seat-off by force plate  
 69 (CFP03000A, Leprino) were measured simultaneously,  
 70 and the association between them and the seat-off pa-  
 71 rameter's width were examined (Fig. 2).



72  
 73  
 74 Figure 1 Definition of COG-heel horizontal distance  
 75 and COG horizontal velocity



76  
 77 Figure 2 Motion capture systems and Floor reaction  
 78 force plate

79  
 80 Seat-off parameters were created by COG-heel hori-  
 81 zontal distance and the COG horizontal velocity of the  
 82 mean value of the fastest and slowest rising speed over

1 the five attempts. Fig. 3 shows the definition of  
 2 seat-off parameters and the distribution of seat-off pa-  
 3 rameters. The horizontal axis was the width of  
 4 COG-heel horizontal distance of the width, and the ver-  
 5 tical axis was the width of the COG horizontal velocity.  
 6 The visual distribution of the visual seat-off parameters  
 7 were attempted to grasp the longitudinal balancing capa-  
 8 bility at the seat-off. For the floor reaction force at  
 9 seat-off, the average value of the floor reaction force  
 10 horizontal and vertical components of the fastest and  
 11 the slowest of the five attempts were calculated for  
 12 each subject.

13 In addition, these average values were plotted on a  
 14 graph where the horizontal axis was the width of the  
 15 floor reaction force horizontal component( $F_y - F'y$ ),  
 16 and the vertical axis was the width of the floor reaction  
 17 force vertical component( $F_z - F'z$ ) during the slowest  
 18 and fastest attempts. The relation between seat-off pa-  
 19 rameters was analyzed, and the longitudinal balancing  
 20 ability at seat-off was verified mechanically(Fig. 4).

### 3. Results

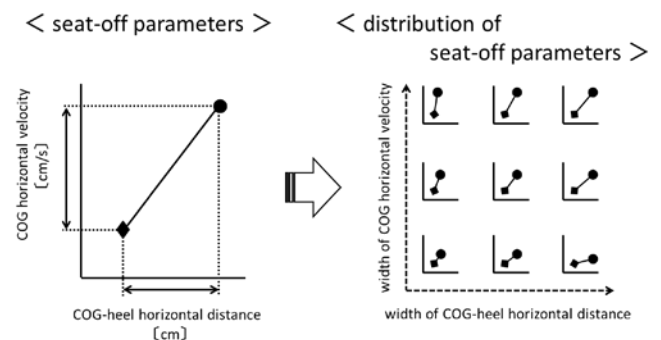
23 The seat-off parameters of all subjects are shown in Fig.  
 24 5. The distribution of seat-off parameters are shown in  
 25 Fig. 6. The results of examining the distribution of the  
 26 seat-off parameters, showed that the unstable rising  
 27 group went through the stable rising group, and was  
 28 symmetrically distributed into a 5 person group and a 4  
 29 person group. This result was reflected in the distribu-  
 30 tion into a form which is supported by the experimental  
 31 results from the floor reaction force distribution by mo-  
 32 tion analysis (Fig. 7).

33 The 5 person group in the upper left hand corner  
 34 were defined as unstable rising group A, and the 4 per-  
 35 son group distributed to the right bottom were defined  
 36 unstable rising group B. Including the stable rising  
 37 group, the three groups in the task were compared and a  
 38 comparison of the floor reaction force measurement  
 39 value of the width of the seat-off parameters was car-  
 40 ried out (Table 1, Table 2). For the width of the seat-off  
 41 parameters in the three groups, the width of the  
 42 COG-heel horizontal distance at seat-off was compared  
 43 using an analysis of variance among the three groups,  
 44 and no significant difference among the three groups  
 45 was found.

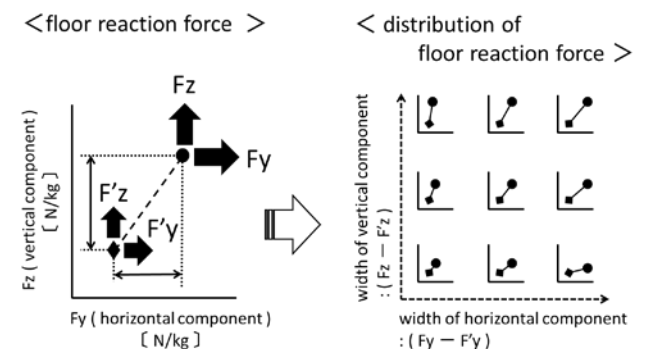
46 Since the COG horizontal velocity width was sig-  
 47 nificantly different among the three groups, the results  
 48 were compared using the Ryan method and the unstable  
 49 rising group was found to have a significantly smaller  
 50 velocity than the other two groups. The results of the  
 51 comparison of the floor reaction forces among 3 groups  
 52 was performed and shown below:

53 Since the  $F_y$  component force for the fastest task  
 54 varied significantly between the three groups, the re-  
 55 sults were compared using the Ryan method. It was  
 56 found that the force was significantly greater for unsta-

57 ble standing group A than for the other two groups.  
 58 Since the  $F_z$  component force for the fastest task was  
 59 significantly different between the three groups, the  
 60 results were also compared using the Ryan method The  
 61 component force was found to be significantly greater  
 62 in unstable standing group B than in the other two  
 63 groups. Since the  $F_y$  component force for the slowest  
 64 task was significantly different among the three groups.  
 65 The force was significantly greater for unstable stand-  
 66 ing group B than for the other two groups. As for the  $F_z$   
 67 component force for the slowest task, it was not found  
 68 to be significantly different among the three groups  
 69 (Table 1, 2).



70  
 71 Figure 3 Schematic diagram of seat-off parameters and  
 72 the distribution at the seat-off



73  
 74  
 75 Figure 4 Schematic diagram of floor reaction force  
 76 and the distribution at the seat-off

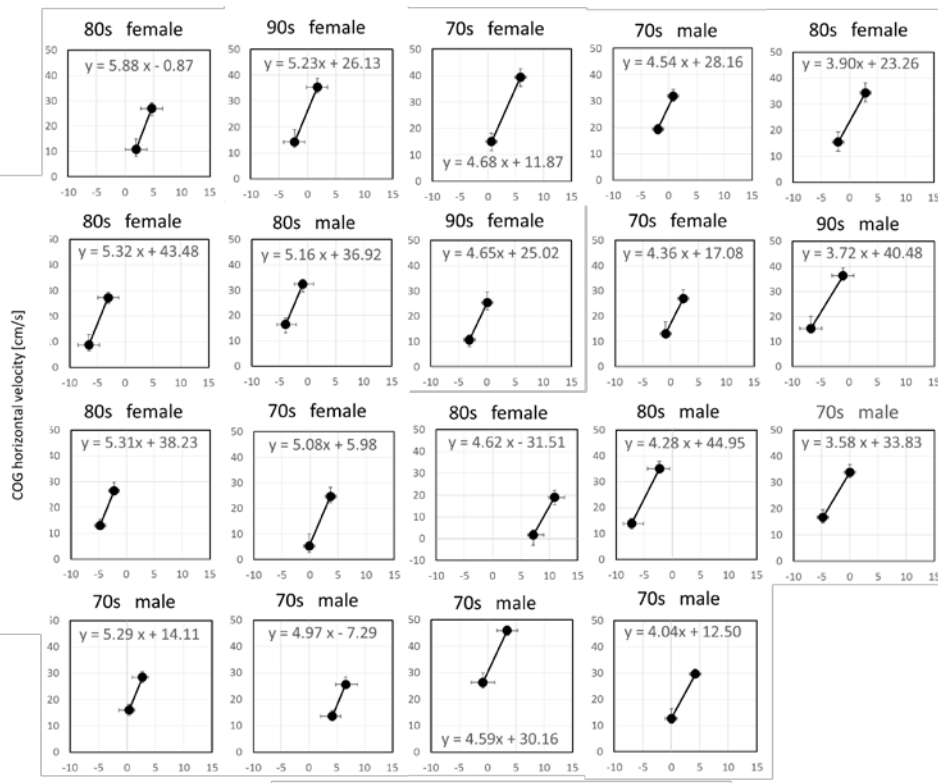
77  
 78 Table 1 Width of seat-off parameters at the seat-off

	width of COG-heel horizontal distance	width of COG horizontal velocity
unstable rising group A	2.29 ± 0.16	18.54 ± 1.03
unstable rising group B	4.47 ± 0.33	13.03 ± 1.04*
stable rising group	3.78 ± 0.97	17.21 ± 3.38

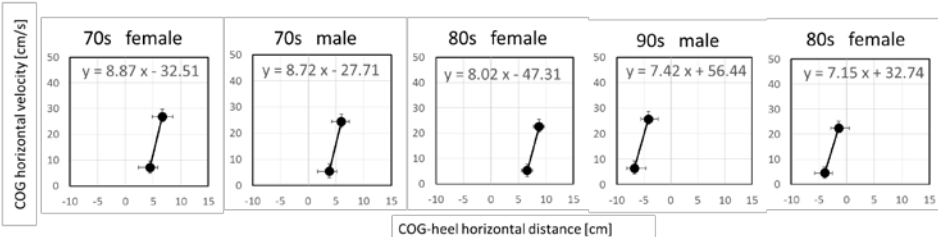
width of COG-heel horizontal distance : average[ cm ]±SD,  
 width of COG horizontal velocity : average[ cm/s ]±SD p<0.01

80  
 81  
 82 Table 2 Floor reaction force at the seat-off

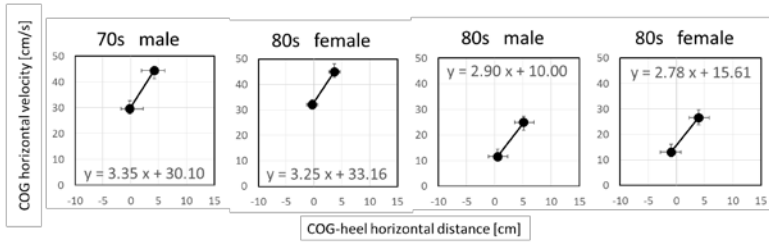
	at fastest		at slowest	
	$F_y$	$F_z$	$F_y$	$F_z$
unstable rising group A	0.29 ± 0.02*	1.18 ± 0.02	0.12 ± 0.04	1.07 ± 0.01
unstable rising group B	0.22 ± 0.08	1.28 ± 0.04*	0.19 ± 0.01*	1.05 ± 0.03
stable rising group	0.19 ± 0.02	1.23 ± 0.02	0.14 ± 0.03	1.07 ± 0.02



(a) stable rising group

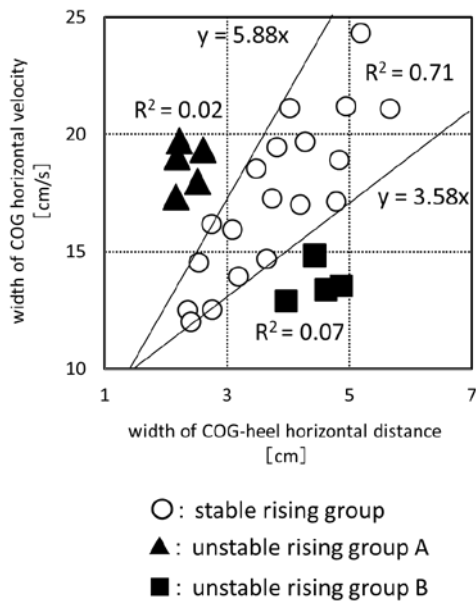


(b) unstable rising group A

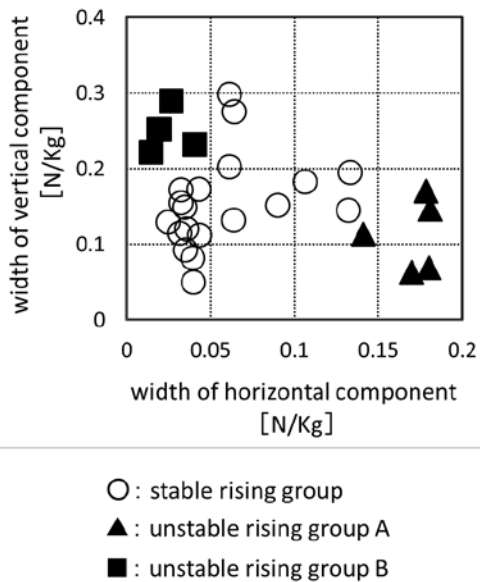


(c) unstable rising group B

Figure 5 Seat-off parameters of all subjects



1  
2 Figure 6 Distribution of seat-off parameters of all sub  
3 jects  
4



5  
6  
7 Figure 7 Distribution of floor reaction forces of all sub  
8 jects

#### 4. Discussion

11 The inclination of the distribution of the seat-off pa-  
12 rameters for the stable rising group (9 males, 10 fe-  
13 males) converged within a certain range. The inclina-  
14 tion of the distribution of the seat-off parameters for the  
15 remaining two groups (4 males, 5 females) deviated  
16 from this range, especially in those who had more than  
17 two fall experiences in the survey taken during the past  
18 year. In the stable rising group, while a strong positive  
19 correlation was observed between the COG-heel hori-  
20 zontal distance width and the COG horizontal velocity  
width, a correlation was not observed in the unstable

22 rising group. In this experiment, when analyzing the  
23 results of the distribution of seat-off parameters of the  
24 three groups, including the corresponding property was  
25 found to be necessary for changes in rising speed.

26 In the stable rising group, it was presumed that at  
27 seat-off, in order to obtain stability corresponding to the  
28 rising speed, the COG horizontal velocity must be con-  
29 trolled by adjusting the COG-heel horizontal distance  
30 and stabilizing the body by governing the COG position  
31 within the supporting basal plane. Additionally, as the  
32 seat-off parameters are distributed in the lower left re-  
33 gion, if the distance between the slowest and fastest is  
34 short, it means that the possible range of rising actions  
35 is very limited. Conversely, the greater the seat-off pa-  
36 rameters are distributed in the upper right, and if the  
37 slowest to fastest distance is long, it means that the  
38 possible range of rising actions is very broad.

39 On the other hand, the disturbed balance of  
40 COG-heel horizontal distance and COG horizontal ve-  
41 locity during seat-off in the unstable rising may not act  
42 reciprocally, and it is inferred that this is the cause of  
43 the instability. In other words, when the COG-heel hori-  
44 zontal distance and the COG horizontal velocity vary  
45 while maintaining a proportional relationship within a  
46 fixed range, this mechanism leads to stability in rising.  
47 However, when deviated from, rising becomes unstable.  
48 From the fact that the distribution of seat-off param-  
49 eters for the unstable rising group A had been displaced  
50 into the upper left side of the stable rising group, it was  
51 inferred to have a tendency of being excessively de-  
52 pendent on the COG horizontal velocity in order to re-  
53 spond to changes in rising speed.

54 Similarly, the distribution of seat-off parameters  
55 for unstable rising group B had been displaced into the  
56 lower right side of the stable rising group, and it was  
57 inferred to have a tendency of being excessively de-  
58 pendent on the COG-heel horizontal distance in order  
59 to respond to changes in standing speed. The distribu-  
60 tion of the experimental seat-off parameters of the sta-  
61 ble rising group, was within the range of  $y = 5.88x$  and  
62  $y = 3.58x$ , the seat-off parameters of unstable rising  
63 group A and unstable rising group B deviated from this  
64 range.

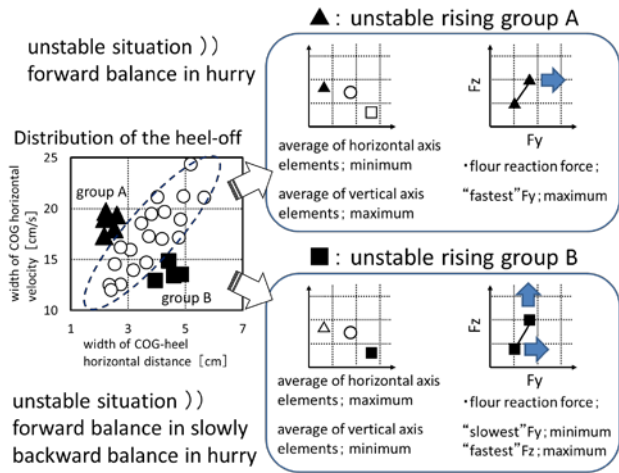
65 In addition, the potential characteristics at the time  
66 of rising for the unstable rising group were analyzed  
67 from the width of the seat-off parameters and the floor  
68 reaction force values. The seat-off parameters of unsta-  
69 ble rising group A (2 males, 3 females) had the mini-  
70 mum COG-heel horizontal distance width among the  
71 three groups, and the largest COG horizontal velocity  
72 width among the three groups. For the floor reaction  
73 force, the  $F_y$  component force at the time of fastest task  
74 was significantly larger than that of the other two  
75 groups.

76 Therefore, it was inferred that unstable rising  
77 group A has a tendency for its balance to collapse in a  
78 forward direction, especially when attempting to rise  
79 quickly. Among the three groups, the seat-off param-



1 ters of unstable rising group B (2 males and 2 females)  
 2 exhibited the maximum COG-heel horizontal distance  
 3 width and the minimum COG horizontal velocity width.  
 4 In addition, the Fz component force when performing  
 5 the fastest task and the Fy component force when per-  
 6 forming the slowest task were significantly greater than  
 7 the other two groups. From these results, it was pre-  
 8 sumed there is a tendency such as the following:

9 In unstable rising group B, when rising particular-  
 10 ly quickly, balance in the rear direction is likely to col-  
 11 lapse, and forward balance is likely to collapse when  
 12 attempting to rise slowly(Fig. 8).



13  
 14 Figure 8 Features of instability at the time of standing  
 15 of the 2 unstable rising groups

16  
 17 **5. Conclusion**  
 18

19 An evaluation of longitudinal balancing capacity during  
 20 rising in the elderly was attempted as follows:

- 21 (1)Seat-off parameters consisting of the COG-heel hori-  
 22 zontal distance and COG horizontal velocity at seat-off  
 23 were created.
- 24 (2)By analyzing the distribution of seat-off parameters,  
 25 longitudinal balancing ability was able to be grasped.
- 26 (3)Floor reaction forces at the time of seat-off were  
 27 verified.

28 As a result, elderly subjects exhibiting instability  
 29 during rising were divided into two groups, and the  
 30 following characteristics were revealed at the time of  
 31 each rising behavior.

32 (1)Unstable balance in the forward direction-types:  
 33 there was instability in forward balance, especially  
 34 when attempting to rise in a hurry.

35 (2)Unstable balance in the rear direction-type: instabil-  
 36 ity exists in backward balance when attempting to rise  
 37 up in a hurry, and instability in forward balance when  
 38 trying to rise slowly.

39  
 40

41 **References**

42  
 43 [1] Ministry of Health, Labour and Welfare: The  
 44 comprehensive survey of living conditions 2014.  
 45 [2] Kannus P, Palvanen M, Niemi S, Parkkari J, Natri  
 46 A, Vuori I, Järvinen M: Increasing number and  
 47 incidence of fall-induced severe head injuries in  
 48 older adults : nationwide statistics in Finland in  
 49 1970-1995 and prediction for the future. Am J  
 50 Epidemiol. 149, pp. 143-150, 1999.  
 51 [3] Kanae K, Ryoko K, Yumi H, Manami T, Yuko N,  
 52 Yasuo N: Prognostic validity of executive func-  
 53 tion and injurious fall history in evaluating inju-  
 54 rious fall risk among frail elderly people, Journal  
 55 of rehabilitation and health sciences. 8, pp. 23-28,  
 56 2010.(in japease)  
 57 [4] Leveille SG, Penninx BW, Melzer D, Izmirlian  
 58 G,Guralnik JM: Sex differences in the prevalence  
 59 of mobility disability in old age: the dynamics of  
 60 incidence, recovery and mortality. J Gerontol B  
 61 Psychol Soc Sci. 55, pp. 41-50, 2000.  
 62 [5] Brooks SV, Faulkner JA: Skeletal:muscle weak-  
 63 ness in old age underlying mechanisms. Med Sci  
 64 Sports Exerc. 26, pp. 432-439, 1994.  
 65 [6] Sieri T, Baretta G: Fall risk assessment in very old  
 66 and females living in nursing homes. Disabil Re-  
 67 habil. 12(12), pp. 718-723, 2004.  
 68 [7] Tinetti ME, Speechley M, Ginter SF. Risk factors  
 69 for falls among elderly persons living in the  
 70 community.N Engl J Med. 319, pp. 1701-1706,  
 71 1988.  
 72 [8] Tinetti ME, Richman D, Powell L: Falls efficacy  
 73 as a measure of fear of falling. J Gerontol. 45, pp.  
 74 239-243, 1990.  
 75 [9] Tinetti ME, Mendes de Leon CF, Doucette JT: Fear  
 76 of falling and fall-related efficacy in relationship  
 77 to functioning among community-living elders. J  
 78 Gerontol. 49(3), pp. 140-147, 1994.  
 79 [10] Kinugasa T, Nagasaki H, Ito H, Hashizume H,  
 80 Furuna T, Maruyama H: Effect of aging on motor  
 81 ability in men aged 18 to 83 years, jpn. J. phys.  
 82 Fitness sports Med. 43, pp. 343-351, 1994.  
 83 [11] Arai T, Shiba Y, Watanabe S, Shibata H: The rela-  
 84 tionship between the stride time variability, motor  
 85 ability and fall in community-dwelling elderly  
 86 people. Japanese Physical Therapy assosiasion.  
 87 38(3), pp. 165-172, 2011.  
 88 [12] Burdett RG, Habasevich R, Pisciotta J. Biome-  
 89 chanical comparison of rising from two types of  
 90 chair. Phys Ther. 65, pp. 1177-1183, 1985.  
 91 [13] Vander LDW, Brunt D, McCulloch MU: Variant  
 92 and invariant characteristics of the sit-to-stand  
 93 task in healthy elderly adults. Arch Phys Med  
 94 Rehabil. 75, pp. 653-660, 1994.  
 95 [14] Alexander NB, Schultz AB, WarWick DN; Rising  
 96 from a chair: Effects of age and functional abli-  
 97 lity on performance biomechanics. J Geronto1. 46,  
 98 pp. 91- 98, 1991.

- 1 [15] Schenkman M, Riley PO, Pieper C: Sit to stand  
2 from progressively lower seat heights—alterations  
3 in angular velocity. *Clin Biomech* 11. 3, pp.  
4 153-158, 1996.
- 5 [16] Shumway Cook A, Woollacot Mt H: Motor con-  
6 trol. lippincot Wtilliams&Wilkins. pp. 4-5, 2007.
- 7 [17] Schenkman ML, Berger RA, Riley PO:  
8 Whole-body movements during rising to standing  
9 from sitting, *Phys Ther.* 70(10), pp. 638-648,  
10 1990.
- 11 [18] Hughes MA, Weiner DK, Schenkman ML et  
12 al. :Chair rise strategies in the elderly *Clin Bio-*  
13 *mech.* 9, pp. 187-192, 1994.
- 14